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# Comparative dosimetrical analysis of intensity-modulated arc therapy, CyberKnife therapy and image-guided interstitial HDR and LDR brachytherapy of low risk prostate cancer

**RESEARCH PAPER** 

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### ABSTRACT

**Background:** The objective of the study was to dosimetrically compare the intensity-modulated-arc-therapy (IMAT), Cyber-Knife therapy (CK), single fraction interstitial high-dose-rate (HDR) and low-dose-rate (LDR) brachytherapy (BT) in low-risk prostate cancer.

**Materials and methods:** Treatment plans of ten patients treated with CK were selected and additional plans using IMAT, HDR and LDR BT were created on the same CT images. The prescribed dose was 2.5/70 Gy in IMAT, 8/40 Gy in CK, 21 Gy in HDR and 145 Gy in LDR BT to the prostate gland. EQD2 dose-volume parameters were calculated for each technique and compared.

**Results:** EQD2 total dose of the prostate was significantly lower with IMAT and CK than with HDR and LDR BT, D90 was 79.5 Gy, 116.4 Gy, 169.2 Gy and 157.9 Gy (p < 0.001). However, teletherapy plans were more conformal than BT, COIN was 0.84, 0.82, 0.76 and 0.76 (p < 0.001), respectively. The D<sub>2</sub> to the rectum and bladder were lower with HDR BT than with IMAT, CK and LDR BT, it was 66.7 Gy, 68.1 Gy, 36.0 Gy and 68.0 Gy (p = 0.0427), and 68.4 Gy, 78.9 Gy, 51.4 Gy and 70.3 Gy (p = 0.0091) in IMAT, CK, HDR and LDR BT plans, while D<sub>0.1</sub> to the urethra was lower with both IMAT and CK than with BTs: 79.9 Gy, 88.0 Gy, 132.7 Gy and 170.6 Gy (p < 0.001). D<sub>2</sub> to the hips was higher with IMAT and CK, than with BTs: 13.4 Gy, 20.7 Gy, 0.4 Gy and 1.5 Gy (p < 0.001), while D<sub>2</sub> to the sigmoid, bowel bag, testicles and penile bulb was higher with CK than with the other techniques.

**Conclusions:** HDR monotherapy yields the most advantageous dosimetrical plans, except for the dose to the urethra, where IMAT seems to be the optimal modality in the radiotherapy of low-risk prostate cancer.

**Key words:** prostate cancer; intensity-modulated arc therapy; Cyberknife therapy; interstitial high-dose-rate brachytherapy; interstitial low-dose-rate brachytherapy

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# Introduction

Prostate cancer is the second most common cancer in men worldwide and the fourth most commonly occurring cancer overall. There were 1.3 million new cases in 2019. It is estimated that 33,000 deaths from this disease will occur this year [1]. The standard of care in the curative treatment of lowand selected intermediate-risk prostate cancer is external beam radiotherapy with intensity-modulated arc therapy (IMAT) or with CyberKnife (CK) technique or interstitial high-dose-rate (HDR) or low-dose-rate (LDR) brachytherapy (BT) [2].

Since the  $\alpha/\beta$  value of prostate tumour is low, dose escalation has an essential role in the development of all radiotherapy modalities [3–5]. The

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more complex the techniques, the more capable they are of escalating the dose to the tumour, while sparing the organs at risk (OARs). The IMAT technique results improved OAR sparing with acceptable planning target volume (PTV) coverage [6]. Stereotactic radiotherapy with CyberKnife demonstrated favourable tumour control, better patient reported quality of life and lower levels of toxicity [7]. The use of BT, as a boost, has been linked with improved biochemical progression free and overall survival [8, 9]. What is more, modern LDR monotherapy approach results in improved quality of life, as a consequence of lower acute urinary and rectal toxicity [11], with the dose coverage of the target volume (D90, the minimum dose delivered to 90% of the prostate) correlating with local tumour control [11], and the dose of the most exposed part of the OARs with normal tissue toxicity [12].

Despite the wide-spread application of these state-of-the-art techniques, no detailed analysis of all of these treatment techniques exists. Leszczyński et al. compared the dose distributions of intensity modulated prostate radiotherapy versus the IMAT technique [13]. Yang et al. investigated the dosimetric differences among IMAT, HDR and LDT BT for 10 patients, but HDR BT was not a single fraction monotherapy in their study [14]. Andrzejewski et al. studied the feasibility of dominant intraprostatic lesion (DIL) boosting using IMAT, proton therapy or HDR BT for 12 patients [15]. Georg et al. examined the optimal radiotherapy technique among IMAT, proton-, carbon-ion therapy and HDR or LDR BT, but HDR BT was not a single fraction monotherapy for the 10 studied patients [2]. Morton et al. studied HDR and LDR BT techniques against IMAT external beam therapy [16]. Fuller et al. dosimetrically compared CK and HDR BT plans for their first 10 patients treated with CK, but not all of the OARs relevant to CK treatment were evaluated [17]. King examined HDR versus LDR BT as monotherapy and boost in a radiobiological model [18]. Skowronek made a practical comparison between HDR and LDR prostate BT [19].

At our institute, all of the four widely used treatment techniques are available. To take the advantage of this situation, the aim of the present study is a detailed dosimetric comparison of intensity-modulated arc therapy, CyberKnife therapy, interstitial high-dose-rate and low-dose-rate brachytherapy, as monotherapy in low-risk prostate cancer.

# Materials and methods

Ten CK plans of patients with organ confined prostate cancer treated at our institute were included in this study. Selection criteria for treatment were the following: PSA < 15 ng/mL and/or GS  $\leq$  7 and/or Stage T  $\leq$  2c [20].

CK treatments were performed with non-coplanar fields using CyberKnife M6 linear accelerator (Accuray, Sunnyvale, CA, USA). Gold fiducial markers were implanted into the prostate gland to guide the placement of radiation beams during treatment. The CTV was extended by an isotropic 3 mm margin, 8 Gy was delivered to this prostate PTV in each fraction according to an ongoing phase II prospective trial in our institute. A total of 5 fractions (total dose 40 Gy) were given every second working day. For treatment planning Accuray Precision 1.1 treatment planning system (TPS) (Accuray, Sunnyvale, CA, USA) was used. The dose was prescribed to the 80-85% isodoses (Fig 1B). The relative volume of the PTV receiving at least the prescribed dose (V100) had to be at least 95%. The detailed description of our treatment method can be found in our previous publication [21].

On the CT series made for CK treatment planning, additional plans using IMAT, HDR and LDR BT were created using the same contour set. Where urethra was not identifiable on CT images, it was contoured between the bladder and the penile channel using a 15 mm pearl. IMAT plans were made in Eclipse v13.7 TPS (Varian Medical Systems, Palo Alto, USA) with a beam energy of 10 MV using 2 full arcs (Fig. 1A). CTV was extended using an isotropic 5 mm margin. The prescribed dose was 70 Gy, the dose of the daily fractions was 2.5 Gy for the PTV [22]. The protocol of our PROMOBRA study was applied for treatment planning in both HDR and LDR BT plans [23]. The prescribed dose in HDR BT was 21 Gy (V100  $\ge$  95%) to the CTV of the CK plan, as the BT PTV, in a single treatment fraction using Ir-192 radioactive source. HIPO method was used to optimize the plans in the Oncentra Prostate v3.1 TPS (Elekta Brachytherapy, Veendendaal, The Netherlands) (Fig. 1C). In LDR BT the prescribed dose was 145 Gy (V100  $\ge$  95%) to the same CTV. IPSA optimisation method in the Oncentra Prostate v3.1 TPS (Elekta Brachy-



**Figure 1.** Axial CT slide (left) and 3D reconstruction (right) of a prostate intensity-modulated arc therapy (**A**), CyberKnife (**B**), an interstitial high-dose-rate prostate brachytherapy (**C**) and an interstitial low-dose-rate prostate brachytherapy plan (**D**). Red: prostate, yellow: prostatic urethra, light green: bladder, brown: rectum, dark brown: sigmoid, khaki: bowel bag, slate blue: femoral heads, lavender: penis, purple: penile bulb, orange: testicles

therapy, Veendendaal, The Netherlands) was used to calculate the virtual positions of the I-125 isotopes (Fig. 1D). The detailed description of our treatment method can be found in our previous publications [24–27].

The equivalent dose given in 2 Gy fractions (EQD2) was calculated for each technique using the linear-quadratic radiobiological model [28, 29]. The  $\alpha/\beta$  of prostate was assumed 1.5 Gy, while for OARs 3 Gy was used [30, 31]. 1 year was estimated in LDR BT as overall treatment time, as during this time 89% of the prescribed dose is delivered. The

following dose-volume parameters were used for quantitative evaluation of plans:

- D90: the minimum dose delivered to 90% of PTV (Gy);
- COIN: conformal index [32];
- D<sub>0.1</sub>(x), D<sub>2</sub>(x): the minimal dose of the most exposed 0.1 and 2 cm<sup>3</sup> of the critical organ x (Gy), where x: rectum (r), urethra (u), bladder (b), hips (h), sigmoid (s), bowel bag (bb), testicles (t) and penile bulb (p).

Friedman ANOVA and Fisher-LSD (Least Significant Difference) post-hoc tests were used (Sta-

EQD2	IMAT	СК	HDR	LDR	p*	**post hoc
D90 [Gy]	79.5	116.4	169.2	157.9	< 0.001	IMAT, CK
COIN	0.84	0.82	0.76	0.76	< 0.001	IMAT-LDR, HDR
D <sub>0.1</sub> (r) [Gy]	86.4	80.0	55.3	93.5	0.0280	HDR, LDR
D <sub>2</sub> (r) [Gy]	66.7	68.1	36.0	68.0	0.0427	HDR
D <sub>0.1</sub> (u) [Gy]	79.9	88.0	132.7	170.6	< 0.001	All
D <sub>2</sub> (b) [Gy]	68.4	78.9	51.4	70.3	0.0091	HDR
D <sub>0.1</sub> (h) [Gy]	17.3	26.5	0.6	2.1	< 0.001	IMAT, CK
D <sub>2</sub> (h) [Gy]	13.4	20.7	0.4	1.5	< 0.001	IMAT, CK
D <sub>0.1</sub> (s) [Gy]	1.3	20.7	0.9	3.8	< 0.001	СК
D <sub>2</sub> (s) [Gy]	1.1	17.9	0.8	2.8	< 0.001	СК
D <sub>0.1</sub> (bb) [Gy]	1.1	12.1	1.1	1.3	< 0.001	СК
D₂(bb) [Gy]	0.9	11.2	0.7	0.8	< 0.001	СК
D <sub>0.1</sub> (t) [Gy]	0.4	23.0	0.7	4.7	0.0006	CK, LDR
D <sub>2</sub> (t) [Gy]	0.4	20.7	0.6	4.2	0.0017	CK, LDR
D <sub>0.1</sub> (p) [Gy]	15.2	23.7	3.2	5.0	0.0014	IMAT, CK
D <sub>2</sub> (p) [Gy]	4.9	10.3	1.7	3.2	0.0057	IMAT, CK

**Table 1.** Mean EQD2 total doses of intensity-modulated arc therapy (IMAT), CyberKnife (CK), high-dose-rate (HDR) and low--dose-rate (LDR) brachytherapy of prostate cancer. D90: the minimum dose delivered to 90% of prostate, COIN: conformal index,  $D_{0.1}(x)$ ,  $D_2(x)$ : the minimal dose of the most exposed 0.1 and 2 cm<sup>3</sup> of 'x' organ at risk, where x are rectum (r), urethra (u), bladder (b), hips (h), sigmoid (s), bowel bag (bb), testicles (t) and penile bulb (p). \*Friedman ANOVA \*\*Fisher-LSD post-hoc test

tistica 12.5, StatSoft, Tulsa, OK, USA) to compare EQD2 dose-volume parameters of IMAT, CK, HDR and LDR BT techniques.

## Results

The mean volume of the PTV was 105.7 cm<sup>3</sup> (42.2–189.3 cm<sup>3</sup>) in IMAT, 85.5 cm<sup>3</sup> (31.5–159.2 cm<sup>3</sup>) in the CK and 61.8 cm<sup>3</sup> (19.8–126.2 cm<sup>3</sup>) in both BT plans (which is equal to the original CTV) on average. We found that EQD2 total dose of the prostate was significantly lower with IMAT and CK than with HDR and LDR BT, D90 was 79.5 Gy, 116.4 Gy, 169.2 Gy and 157.9 Gy (p < 0.001). However, IMAT and CK plans were more conformal than BT plans, COIN were 0.84, 0.82, 0.76 and 0.76 (p < 0.001).

In our comparison, the  $D_2$  to the rectum and bladder were lower with HDR BT than with IMAT, CK and LDR BT, it was 66.7 Gy, 68.1 Gy, 36.0 Gy and 68.0 Gy (p = 0.0427), and 68.4 Gy, 78.9 Gy, 51.4 Gy and 70.3 Gy (p = 0.0091) in IMAT, CK, HDR and LDR BT plans, while  $D_{0.1}$  to the urethra was lower with both IMAT and CK than with both BT modalities: 79.9 Gy, 88.0 Gy, 132.7 Gy and 170.6 Gy (p < 0.001), respectively.  $D_2$  to the hips was higher with IMAT and CK, than with BTs: 13.4 Gy, 20.7 Gy, 0.4 Gy and 1.5 Gy (p < 0.001), while  $D_2$  was higher to other organs with CK, than with the other techniques: 1.1 Gy, 17.9 Gy, 0.8 Gy and 2.8 Gy (p < 0.001) for the sigmoid; 0.9 Gy, 11.2 Gy, 0.7 Gy and 0.8 Gy (p < 0.001) for the bowel bag; 0.4 Gy, 20.7 Gy, 0.6 Gy and 4.2 Gy (p = 0.0017) for the testicles; and 4.9 Gy, 10.3 Gy, 1.7 Gy and 3.2 Gy (p = 0.0057) for the penile bulb in IMAT, CK, HDR and LDR BT plans. The detailed results can be found in Table 1.

## Discussion

Dose escalation has a fundamental role in the radiotherapy of low- and selected intermediate-risk prostate cancer [3–5]. Several high-tech teletherapy and BT techniques are widely used, such as image-guided and intensity-modulated teletherapy, arc therapy, stereotactic radiotherapy with linear accelerators or CyberKnife and interstitial HDR or LDR BT [2, 3, 6–9, 11, 12]. In the present study, all of the four widely used radiotherapy techniques (IMAT, CK, HDR and LDR BT) were compared dosimetrically using the linear-quadratic radiobiological model.

Although these techniques rapidly developed parallelly, the dosimetrical differences were con-

spicuous from the beginning. Leszczyński et al. have pointed out that the treatment delivery time is significantly reduced using the IMAT technique compared to intensity-modulated radiotherapy [13]. Yang et al. [14] concluded that HDR and LDR BT significantly reduce the dose to the rectum, bladder and femoral heads compared with IMAT. The mean EQD2 dose to the urethra was 80.3 Gy in IMAT, 70.2 Gy in HDR and 104.9 Gy in their LDR BT plans. They stated that for localised prostate cancer, HDR BT provides the advantage in sparing the urethra compared with IMAT and LDR; however, HDR BT was not a single-fraction treatment in this study. Our results are not in agreement with this, the EQD2 dose to the urethra was the lowest in the IMAT plans, D<sub>0.1</sub> was 79.9 Gy. It was higher, 88.0 Gy, with the CK technique, while still higher using HDR or LDR BT: 132.7 Gy and 170.6 Gy (all of the differences are significant). However, it has to be mentioned, that the relative  $D_{0,1}$  dose to the urethra - in proportion to the EQD2 D90 dose - was 100.5% in IMAT, 75.6% in CK, 78.4% in HDR and 108.0% in the LDR plans. In terms of the other OARs sparing, HDR resulted in the lowest dose. This difference between the studies can be explained by the different fractionation and prescribed dose. Yang et al. used 78 Gy physical dose in 39 fractions in IMAT, 34 Gy in 4 fractions in HDR and 145 Gy in 1 fraction in LDR BT plans and calculated only mean dose of the OARs instead of volumetric doses.

Andrzejewski et al. studied the feasibility of DIL boosting and concluded that higher boost doses were achieved using proton therapy compared to IMAT, keeping doses of major OARs at similar levels, but HDR BT was superior to IMAT and proton therapy, both in terms of OAR sparing and boosting of the DIL [15]. EQD2 D50 to DIL were 110.7 Gy, 114.2 Gy and 150.1 Gy in IMAT, proton therapy and HDR BT plans, while the mean dose of the rectal wall was 30.5 Gy, 16.7 Gy and 9.5 Gy, and the mean dose to the bladder wall were 21.0 Gy, 15.6 Gy and 6.3 Gy, respectively. Georg et al. examined the optimal radiotherapy technique in the radiotherapy of localised prostate cancer and stated that HDR and LDR BT techniques were clearly superior in terms of the bladder and rectal wall sparing, in contrast with IMAT, proton- and carbon-ion therapy, with the lowest values for HDR BT [2]. However, they did not examine the dose to the urethra.

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Based on our comparison, also single fraction HDR monotherapy yields the most advantageous plans, except in terms of the dose to the urethra where IMAT proves to be the optimal modality.

Morton et al. investigated HDR BT against LDR BT and IMAT external beam therapy in a clinical point of view [16]. They concluded that HDR BT enables more consistent implant quality than LDR BT, with evidence of lower acute and late toxicity. Higher disease control rates are also reported with HDR monotherapy than with the IMAT technique. These clinical results are in good agreement with our dosimetrical results. HDR BT resulted in the most optimal treatment plans in terms of both dose coverage of the prostate and the dose to OARs, except for the urethra.

Fuller et al. pointed out that urethra dose is lower for virtual CK than for virtual HDR BT plans, suggesting that the CK technique may more effectively limit urethra dose [17]. Bladder maximum point doses were higher with HDR BT, but bladder dose fall-off beyond the maximum dose region was more rapid with this technique than using CK therapy. Our study added a new result to this conclusion, specifically using IMAT the dose to the urethra is lower than CK and both BT modalities.

Based on the radiobiological examination of King, HDR and LDR BT achieve superior tumour control when compared with IMAT using conventional doses, and HDR BT might achieve superior tumour control compared with LDR [18]. This result supports the clinical evidence for equivalent outcomes in localised prostate cancer with either HDR or LDR BT. However, HDR BT dose escalation regimens might be able to achieve higher biological effectiveness and hence improved outcomes in contrast to IMAT. In the same manner, in our plans, higher EQD2 total doses can be reached to the prostate with BT techniques than with external radiation techniques, and this dose is the lowest using IMAT.

Skowronek [19] demonstrated that all available clinical data regarding HDR and LDR BT suggests that they are equally effective, stage for stage, in providing high tumour control rates. The important difference in dosimetric control is that HDR doses can be escalated safely providing such a flexibility that does not exist for LDR BT. Our examination also gave one vote for HDR BT, as the most appropriate technique of dose escalation in prostate radiotherapy. It has to be mentioned, that in our study, the virtual BT plans were made on the planning CT of the CK, and this anatomy is not optimal for BT planning. Furthermore, the EQD2 prescribed dose was higher in both BT techniques than in the IMAT and CK plans, as the recommended, clinically used fractionation was applied in our plans. Despite that, HDR BT proved to be the optimal choice in the aspects of sparing most of the OARs beside dose coverage of the prostate. LDR BT resulted in higher dose to the OARs with approximately equivalent prescribed dose to the prostate.

## Conclusions

Using single fraction HDR and LDR BT, total dose of the prostate is higher than with IMAT or CK techniques and, accordingly, dose to the urethra is also higher with both BT modalities using the recommended fractionation scheme. Dose to the rectum and bladder is lower with HDR BT than with IMAT, CK and LDR BT, while dose to the sigmoid, bowel bag, testicles and penile bulb are higher with CK than using the other examined techniques. Overall, HDR monotherapy yields the most advantageous plans in the radiotherapy of low- and intermediate risk prostate cancer, except in terms of the dose to the urethra where IMAT proves to be the optimal modality.

### Conflict of interest

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