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In-vitro mechanical behavior and in-vivo healing response of a new generation biodegradable-polymer coated thin strut sirolimus eluting stent

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INTRODUCTION

First-generation drug eluting stents (DES) coated with durable polymers reduced rates of restenosis when compared with bare-metal stents. Although DES achieved great results in inhibiting neointimal hyperplasia, the presence of durable polymers was associated with the added risks of stent thrombosis (ST) [1, 2]. Introduction of second-generation DES resulted in reduced rates of ST with preserved low restenosis rates [3]. However, very late stent thrombosis and neoatherosclerosis have been recently observed with second generation DES [2, 4]. Biodegradable polymers DES were designed to reduce local inflammatory and hypersensitivity reactions responsible for delayed arterial healing, which is the primary substrate underlying late ST [5]. Contemporary DES are increasingly used for treatment of complex lesions such as left-

main and long bifurcated segments. Moreover, stent post-dilatation is frequently performed, typically with large over-expansion in the setting of long tapering vessel segment. Therefore, the information regarding overexpansion capabilities of each device is crucial in clinical practice.

In this study, we aim to evaluate *in-vitro* mechanical behavior and *in-vivo* healing response of a new generation biodegradable-polymer coated thin strut sirolimus eluting stent (Alex Stratos, Balton, Warsaw, Poland) against the commercially available previous generation platform (Alex Plus Balton, Warsaw, Poland) and the leading DES (Orsiro, Biotronik, Bülach, Switzerland).

METHODS

Device description

Alex Stratos is a CE mark approved new generation biodegradable polymer-coated sirolimus-eluting stent with a laser-cut cobalt–chromium alloy platform with a wall thickness of 70 μm . It has improved design with open cells for unobstructed side branch access (Figure 1A). Unlike other contemporary DES which typically has two or three designs to cover the entire range of their diameter, Alex Stratos has an individual design every 0.5 mm in diameter which allows more uniform drug distribution (data on file at Balton). The device is covered with a multilayer structure containing a poly-L-lactide polymer and sirolimus in a dose of 1.2–1.4 mg/mm^2 . Proprietary polymer application process allows maintaining polymer integrity during aggressive overexpansion of the stent up to 1.5 mm above nominal diameter (Figure 1B). In this study Alex Stratos was compared in *in-vitro* and *in-vivo* setting with the commercially available previous generation platform Alex Plus which platform is made of a cobalt–chromium alloy with a wall thickness of 70 μm . Alex Plus is covered with the same multilayer structure as Alex Stratos. Both Alex Stratos and Alex PLUS were evaluated in the *in-vitro* setting against leading cobalt–chromium biodegradable polymer-coated sirolimus-eluting stent Orsiro.

In-vitro overexpansion testing

The mechanical behavior of the investigated Alex Stratos and commercially available Alex Plus and Orsiro stent following over-expansion was examined under static conditions. All tested devices were 3.5×15 mm and were deployed *in-vitro* at nominal pressure. Subsequently, over-expansion results for each design was tested with successive post-dilations using a 4.5×12 mm and semi-compliant balloons inflated at 8 atm followed by a 5.0×12 mm non-compliant balloon with a pressure of 18 atm. Post-dilatation was performed on the proximal segment. Final

dilations were repeated on the samples a second time to ensure an optimal expansion of the stent struts. For each individual stent, two samples were deployed. Stent samples were mounted and analyzed using light digital microscopy and evaluated using previously described methodology (Figure 1C) [6].

In-vivo healing study

The study protocol was approved by the Local Ethics Committee for animal research. All animals received a standard of care outlined in the study protocol and in accordance with the act of animal welfare and the “Principles of Care of Laboratory Animals” [7]. In this study either Alex Stratos (n = 11) or Alex Plus (n = 24) were implanted targeting a stent-to-artery ratio of 1.1:1 under online quantitative coronary angiography (QCA) guidance in 35 coronary arteries of 12 swines. Control coronary angiography, optical coherence tomography (OCT) and histological evaluation was performed 28 days following stent implantation. QCA analysis was performed using QAngio XA Software™ 7.1.14.0 (Medis Medical Imaging System, Leiden, Netherlands). OCT images were recorded using the ILUMIEN PCI Optimization System (St. Jude Medical, St. Paul, MN, USA) and the qualitative analyses were performed with the commercial software (ILUMIEN OPTIS, St. Jude Medical, St. Paul, MN, USA). An independent pathology laboratory (AccelLAB, Boisbriand, Canada) conducted the histological evaluation.

Statistical analyses

Statistical analysis was performed using SigmaStat statistical software (version 13.1; Systat Software, San Jose, CA, USA). The normality of the distribution was verified using the Shapiro–Wilk test. Due to skewed distributions, the median (interquartile range) was provided. QCA, OCT, and histological data were analyzed with nonparametric Mann–Whitney test. Differences were only considered significant when the calculated *P* value was <0.05. In-vitro overexpansion evaluation was performed for exploratory purposes and due to small sample size statistical analysis was not performed.

RESULTS AND DISCUSSION

In-vitro overexpansion testing in static conditions demonstrated that all tested stents were able to expand well above their labelled maximal stent diameter using larger post-dilatation balloons. From tested devices only Alex PLUS presented signs of strut fracture (n = 2) when over-expanded at 1.5 mm above nominal diameter (42% overexpansion). This indicates

improvement in the Alex Stratos architecture when compared to the previous generation Alex Plus. Stents are rarely able to achieve minimal lumen diameter equal to the diameter of the balloon used for postdilatation [8]. In the presented study Alex Stratos achieved minimal lumen diameter closest to the balloon expected diameter during postdilatation using 5.0 non-compliant balloon (Alex Stratos 4.98 mm and 5.01 mm vs. Alex Plus 4.82 mm and 4.86 mm vs. Orsiro 4.76 mm and 4.93 mm). The overexpansion capabilities are especially important in the bifurcation setting where significant discrepancy between the distal and proximal diameter is present. Cell opening at nominal diameter appeared to be numerically largest in Alex Stratos when compared to Alex Plus and Orsiro (respectively: 1.32 mm² and 1.34 mm² vs. 1.09 mm² and 1.13 mm² vs. 1.28 mm² and 1.36 mm²) and increased by 125% and 127% in Alex Stratos, 112% and 120% in Alex PLUS and 126% and 130% in Orsiro between nominal pressure deployment and maximal overexpansion. Side branch access is very important especially during treatment of complex lesions such as bifurcations. Improved design of Alex Stratos allowed increase in mean cell opening by almost 10% when compared to the previous generation Alex Plus achieving similar results to the Orsiro stent. Therefore, due to enhanced overexpansion capabilities and greater cell opening Alex Stratos might be better suited for bifurcation interventions including lesions requiring two stent approach when compared to the previous generation Alex Plus. However, due to small sample size and experimental nature of this study, these results must be interpreted with caution.

In-vivo healing response study evaluated the vascular response to Alex Stratos when compared to Alex Plus. The appropriateness of applied methodology was confirmed by comparable balloon-to-artery ratio, vessel and stents sizes during implantation procedure evaluated by QCA. At 1 month, both devices demonstrated comparable late lumen loss (Alex Stratos = 0.13 [0.00–0.40] mm vs. Alex PLUS = 0.10 [0.05–0.28] mm; $P = 0.54$). OCT analysis demonstrated that there was no difference in the stent area between Alex Stratos and Alex Plus (respectively: 8.41 [6.26–9.32] mm² vs. 7.40 [5.97–8.99] mm²; $P = 0.674$) at 28 days follow up. Furthermore, percentage area of stenosis (%AS: Alex Stratos 9.62 [7.20–12.93] % vs. Alex PLUS 10.47 [9.26–12.67] %; $P = 0.899$) were similar between tested stents (Figure 1E). Histological assessment revealed that vascular responses to Alex Stratos were comparable with those to Alex PLUS at 28 days follow up. Morphometric analysis showed no difference in internal elastic lamina or external elastic lamina area between both devices. %AS were numerically smaller in Alex Stratos when compared to Alex PLUS (respectively: 12.1 [9.7–13.3] % vs. 15.2 [8.9–22.8] %; $P = 0.317$) (Figure 1E). There was no difference in inflammation score between tested groups. Fibrin score was numerically higher in the Alex Stratos group but they still remained

at low level and the difference did not reach statistical significance (Alex Stratos 0.52 [0.33–0.81] vs. Alex PLUS 0.22 [0.15–0.46], $P = 0.055$). Furthermore, fibrin score in both tested groups was numerically lower than previously reported preclinical data for other sirolimus as well as everolimus and zotarolimus-eluting stents [9, 10]. Finally, the animal model of in-stent restenosis in healthy coronary arteries used in this study cannot reproduce the complexity of coronary artery disease in humans, therefore the results have to be interpreted with caution.

In summary, the new-generation Alex Stratos demonstrated improved biomechanical behavior to the previous generation platform (Alex Plus) with the results similar to the Orsiro stent. Furthermore, Alex Stratos demonstrated favorable healing profile in the in-vivo setting. Our findings suggest that the new-generation Alex Stratos tested in this study has the potential to improve the performance shown by the current generation Alex Plus by providing a highly biocompatible platform with significantly improved mechanical properties.

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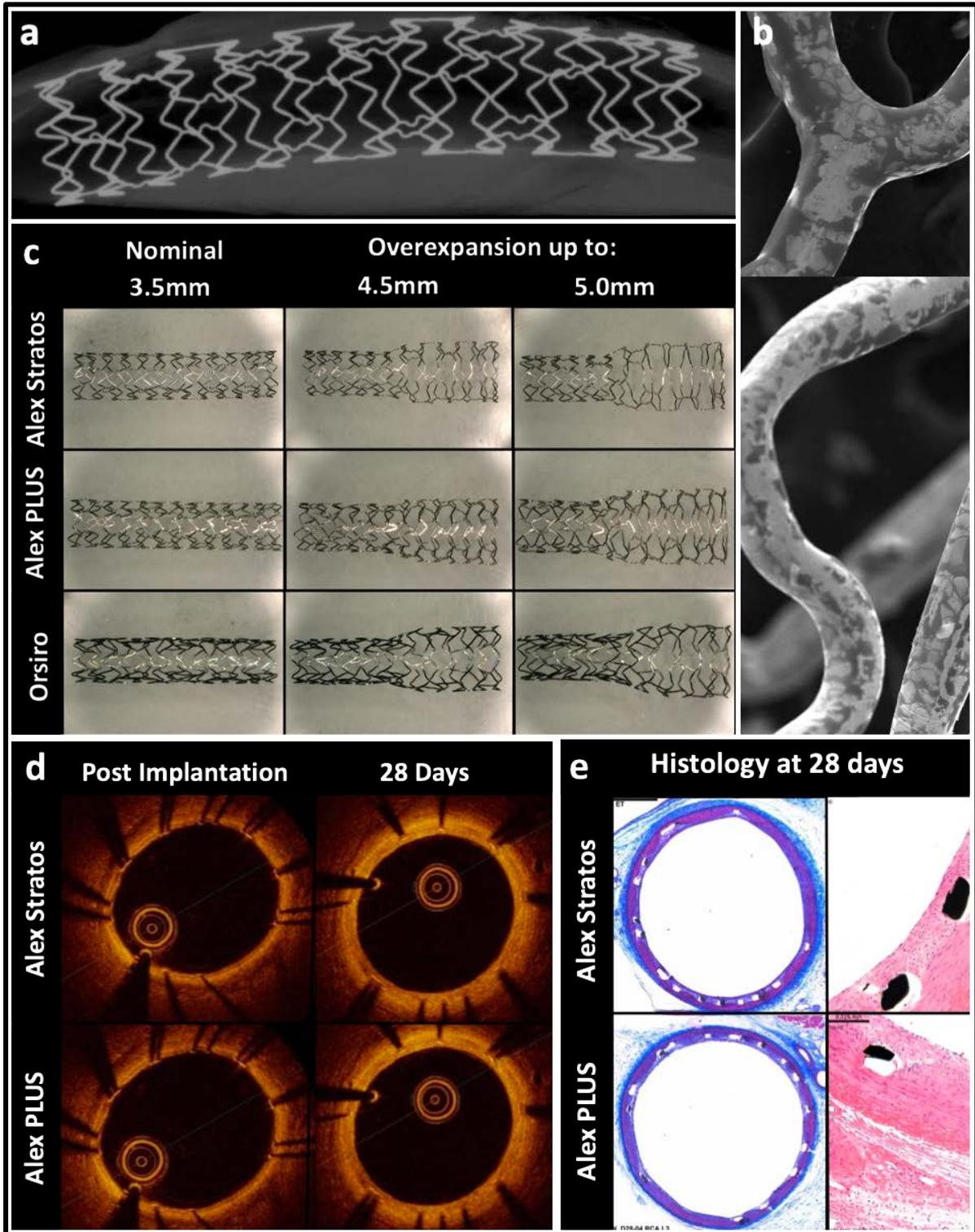


Figure 1. A. High resolution radiography image of Alex Stratos new design with open cells. **B.** Polymer coating integrity after postdilatation 1.5 mm above nominal stent diameter. **C.** Light digital microscopy pictures of Alex Stratos, Alex Plus and Orsiro deployed at nominal diameter (3.5 mm) and postdilatated up to 4.5 mm and 5.0 mm. **D.** Representative optical coherence tomography pictures at 28 days follow up. **E.** Representative histology pictures at 28 days follow up.