

Optimal fluoroscopic viewing angles for stenting of the coronary aorto-ostial lesions

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Abstract

Background: Long-term results after stenting aorto-coronary ostial lesions (AOL) are worse than those achieved in non-ostial locations. AOL interventions still pose a substantial challenge for interventional cardiologists. The aim of the study was to determine the optimal fluoroscopic viewing angles of the left and right coronary ostia, based on multislice computed tomography (MSCT) data.

Methods: Cardiac MSCT exams of 30 patients with clinical suspicion of coronary artery disease were analyzed. En face angles of both coronary ostia, as well as their optimal projection curves, were determined by 2 independent observers in a standard Dicom viewer, without any additional, specialized software add-ons, using a systematic, step-by-step approach. Spatial relations between the ostial plane and the aorta were also assessed.

Results: The average en face angle of the left coronary ostium was RAO 23°, CAU 45°; for the right coronary ostium RAO 18°, CRA 5°. The mean inter-observer differences for the en face angles of the left and right coronary arteries were 5° and 7°, respectively.

Conclusions: Multislice computed tomography data provide precise spatial information on the orientation of the coronary ostia and their relation to the aortic root. Their utilization for determining the patient-specific viewing angle may substantially facilitate percutaneous coronary interventions in AOL. (Cardiol J 2021; 28, 6: 831–841)

Key words: aorto-ostial lesions, coronary intervention, optimal projection curves, multislice computed tomography, cardiovascular imaging

Introduction

Despite constant advances in technology, interventions of the coronary ostia still pose a substantial challenge for interventional cardiologists. Long-term results after stenting of the

aorto-coronary ostial lesions (AOL) are worse than those achieved in non-ostial locations [1, 2]. The gap results partly from differences in the plaque composition, which is more rigid, calcified, and bulky in the case of AOL [3, 4]. A lot of target lesion failures are due to technical problems during

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the procedure, resulting in overly deep stent implantation and incomplete coverage of the treated lesion [5]. On the other hand, excessive protrusion of the stent into the aorta also has negative consequences because it can hinder re-engagement of the vessel with the catheter or seriously complicate subsequent interventions on the aortic valve [6, 7]. Over the last several years, multi-sliced computed tomography (MSCT) has emerged as a useful tool in the assessment of coronary artery disease (CAD) [8–10]. This diagnostic modality offers a unique view into the spatial relationships of different cardiac structures and has been proved to be critical in procedure planning and device selection in structural heart interventions [11–14]. However, three-dimensional (3D) data provided by MSCT are still rarely used to facilitate percutaneous coronary interventions (PCI) [15, 16].

The aim of this study was to determine the optimal fluoroscopic viewing angles for AOL stenting with the use of MSCT examinations of patients with CAD. Patient-specific optimization of the viewing angle can potentially decrease/eliminate parallax error [12] and improve the precision of stent implantation in the coronary ostium. We propose a simple, step-by-step approach to find individually optimized projections with the use of patient MSCT data.

Methods

Setting and image acquisition

Multislice computed tomography examinations of 30 patients with clinical suspicion of CAD were retrospectively analyzed. MSCT was performed according to the established institutional protocol, i.e. in spiral/helical acquisition mode with retrospectively electrocardiogram-gated reconstruction, with a tube voltage of 100–120 kV, and tube current adjusted for patient size. 80–110 mL of contrast was injected into the antecubital vein at a rate of 5 mL/s. The dataset of contrast-enhanced scans was reconstructed in the diastolic phase. Images were reconstructed with a slice thickness of 0.6 mm and a reconstruction interval of 0.4 mm.

Image analysis

Multislice computed tomography exams were then analyzed with a standard DICOM viewer (Osirix Pixmeo SARL, Geneva, Switzerland). A step-by-step approach, described in detail in Figure 1, was used to calculate the *en face* angles of the coronary aorto-ostial orifice plane. Based on the determined *en face* angles, optimal projection

curves (S-curve) (Fig. 2A) were then calculated in an Excel (Microsoft Corporation Redmond, WA, USA) spreadsheet using the following formula described earlier by the Nicolo Piazza group [17]:

$$\emptyset = -\arctan \left[\frac{\cos\theta - \theta_{en\,face}}{\tan \emptyset_{en\,face}} \right]$$

where \emptyset is the cranio-caudal angle of the optimal projection curve at RAO/LAO angle θ , and $\emptyset_{en\,face}$ and $\theta_{en\,face}$ are the cranio-caudal and RAO/LAO angles of the structure viewed *en face*, respectively (online version of the S-curve generator is available at <https://smartheart.pl/plane-calculator/>). The multiplanar reconstruction mode was applied again to define the range of the S-curve in which the adjacent aorta does not overlap with the coronary ostium in the orthogonal angiographic view (Figs. 2B, 3). Each exam was analyzed independently by two cardiologists with experience in cardiac computed tomography (CT) interpretation.

Statistical analysis

En face angles are expressed as mean with 95% confidence interval (CI), taking the average value from both observers. Discrepancies between the investigators were assessed by measuring the average angle between the S-curves produced by each investigator.

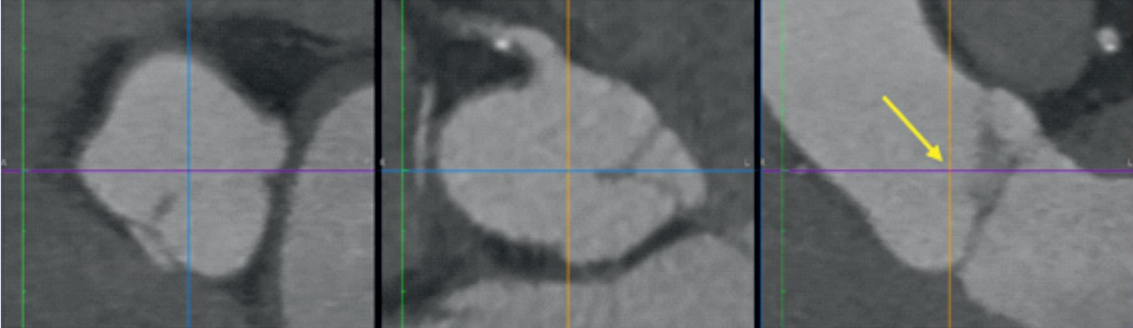
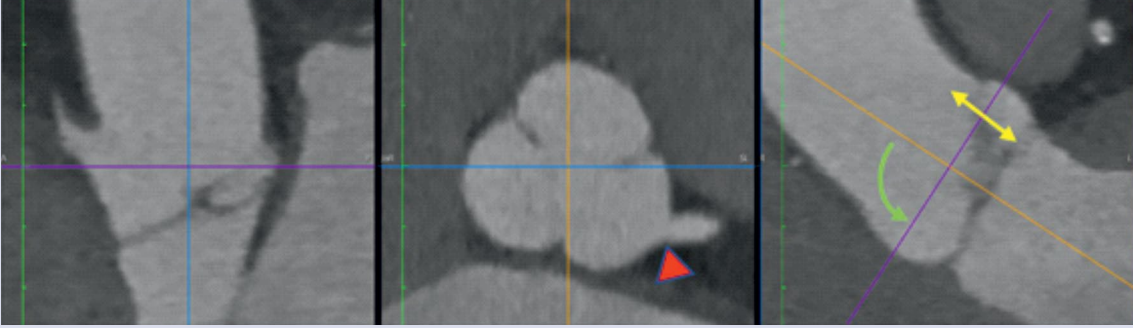
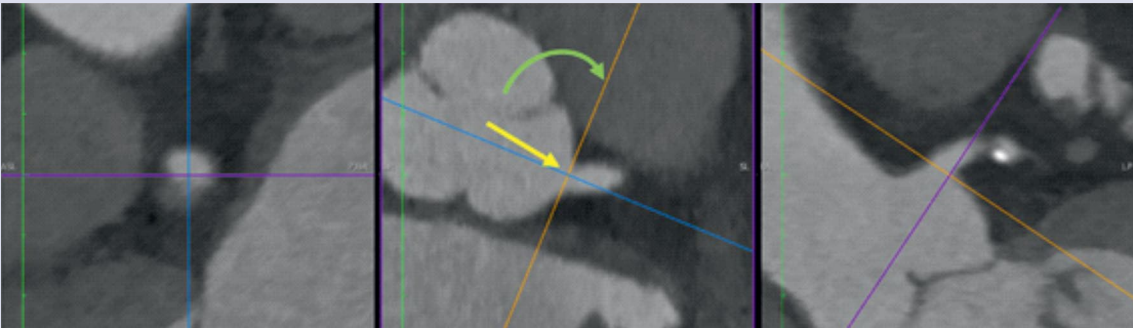
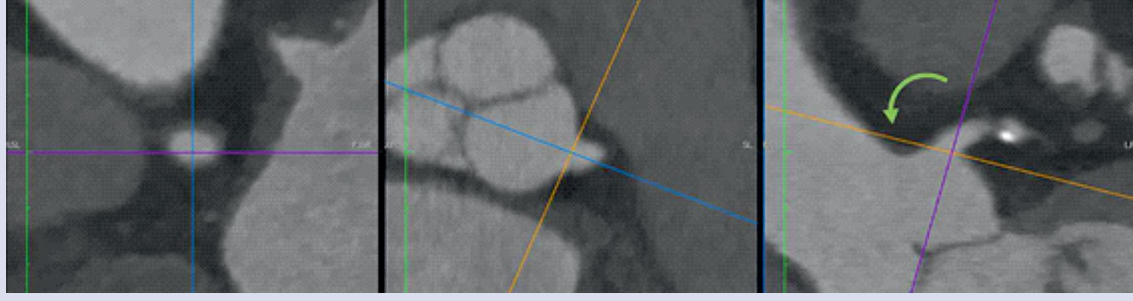
The institutional review board approved the study with a waiver of informed consent.

The numerical data underlying this article and the anonymized CT scan data will be shared on reasonable request to the corresponding author.

Results

Table 1 presents mean *en face* angles of the left and right coronary ostial planes (RAO 29°, CAU 50°; and RAO 18°, CRA 5°, respectively). The mean inter-observer differences for the *en face* angles of the left and right coronary arteries (LCA, RCA) were 5° and 7°, respectively. The average range of the optimal projection curve in which the left coronary ostium does not overlap with the adjacent aorta was RAO 0° to LAO 68°. In the case of the right coronary ostium S-curve, that range was outside of the RAO 37° to LAO 48° zone (Fig. 4).

Figure 5 shows individual projection curves for each patient, the range of “unobstructed” view, and *en face* angles. Mean optimal projection curves, mean “unobstructed” view ranges, and mean *en face* angles for the left and right coronary ostia with 95% CI are presented in Figure 4.

| Sagittal plane | Horizontal plane | Coronal plane |
|--|------------------|---------------|
|  | | |
| <p>Step 1. Place the crosshair at the center of the aortic root (arrow).</p> | | |
|  | | |
| <p>Step 2. In the coronal view window — adjust the horizontal plane (purple line) to be roughly parallel to the aortic annulus (green arrow), then adjust the horizontal plane's position (yellow arrow) to the level of the coronary ostium of interest (red arrowhead).</p> | | |
|  | | |
| <p>Step 3. In the horizontal view window — move the crosshairs to the center of the coronary ostium (yellow arrow), and align the sagittal plane tangentially (green arrow) to the aortic root at the level of the ostium.</p> | | |
|  | | |
| <p>Step 4. In the frontal view window — adjust the sagittal plane tangentially to the aortic root at the level of the ostium (green arrow).</p> | | |

→

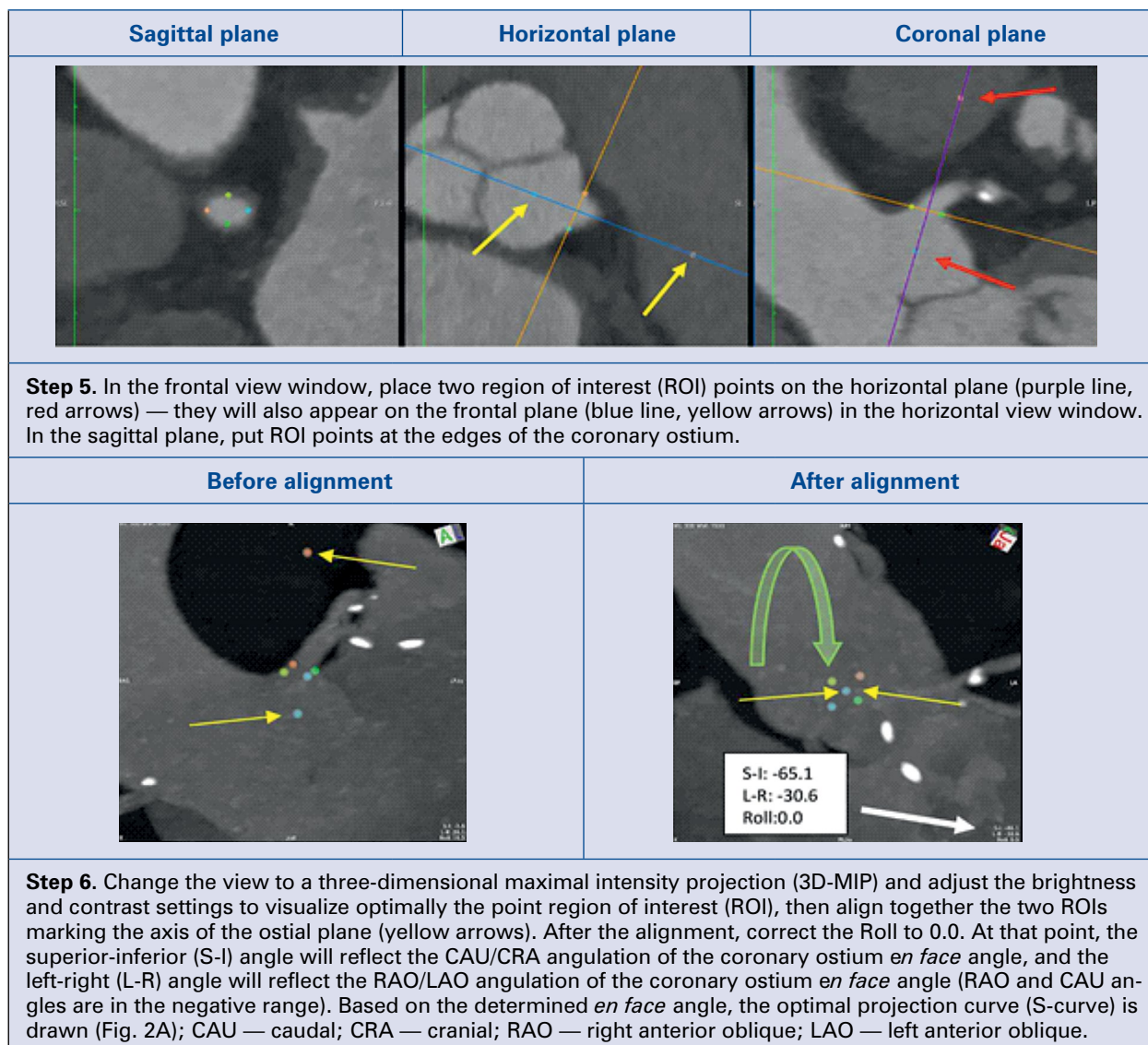


Figure 1. Systematic step-by-step approach for identifying the coronary aorto-ostial plane.

Discussion

The present study determined for the first time the optimal fluoroscopic viewing angles of the LCA and RCA based on MSCT data. This study is interesting from many perspectives: i) first and foremost, we propose a systematic step-by-step approach to determine individual optimal angiographic viewing angles for stenting of the coronary ostia based on patient angio-CT data; and ii) it provides a detailed description of the method, together with a graphic illustration of the concept. Our approach does not need any dedicated software and, thus, can be applied widely in the routine clinical practice.

Percutaneous coronary interventions of aorto-ostial lesions remain challenging

Aorto-ostial lesions are usually defined as coronary artery stenosis greater than 50%, within 3 mm of its origin [18]. They constitute around 3% of all percutaneously treated lesions. The procedural success and clinical outcomes of these lesions are inferior to those of non-ostial locations. The difference results partly from the lesions' distinct plaque composition, causing them to be more bulky, non-compliant, and with a greater tendency towards elastic recoil. The lack of adventitia in the transmural segment may also play a role [2, 3, 19]. However, a suboptimal result is very often caused by the challenges of ostial intervention and imprecise stent positioning.

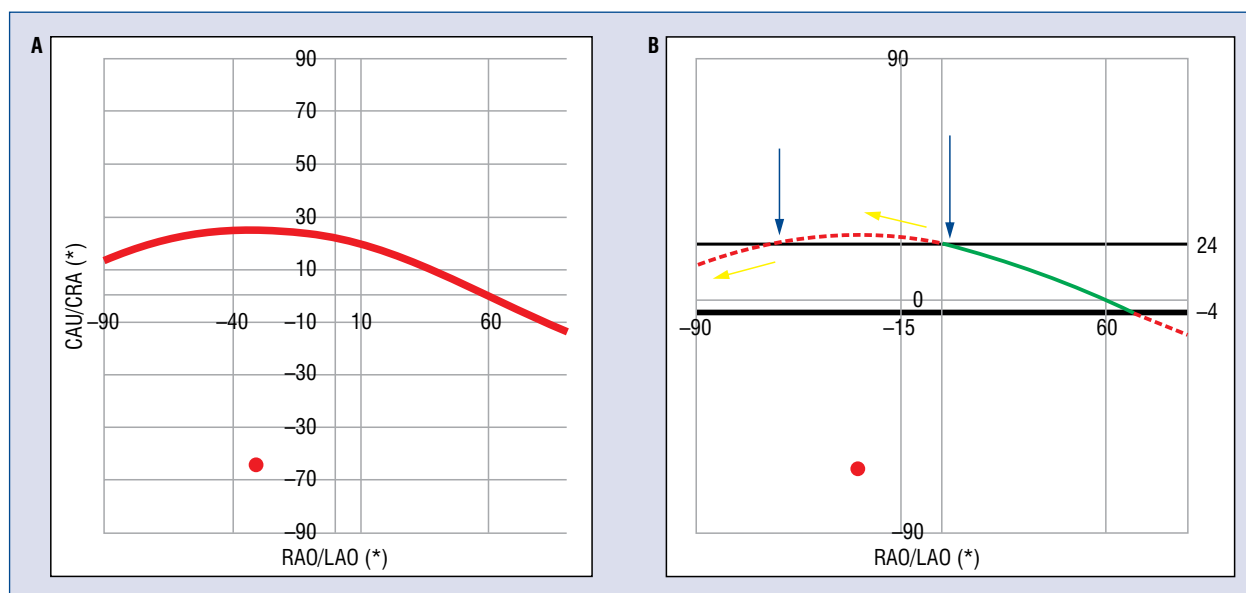


Figure 2. The optimal projection curve based on the determined *en face* angle; **A.** The optimal projection curve (red line) corresponding to the determined *en face* angle of the coronary ostium (red dot); **B.** The range of the optimal projection curve in which the coronary ostium does not overlap with the adjacent aorta. Because determining this range is based on the caudal/cranial (CAU/CRA) angulation, it is crucial to notice that two different points on the S-curve can have the same CAU/CRA angulation value (blue arrows). They can be identified by their relation to the maximal angulation of the curve (yellow arrows). Red dotted lines — “obstructed” view, green line — “unobstructed” view.

The implanted stent of choice in non-ostial lesions is usually long enough to secure a reasonably safe margin on both sides of the lesion and minimize the risk of a geographic miss. In the case of ostial stenoses, one of the margins is completely absent. A deliberate decision to protrude the stent into the aorta may result in many long-term serious consequences. First, the protruding stent makes all subsequent interventions on that vessel much more difficult. It is harder to engage the vessel with the guiding catheter [20], and attempts to do so can deform the protruding struts, potentially increasing thrombotic risk. A recent analysis from the EXCEL trial clearly showed that PCI of a target vessel after left main (LM) stenting was a strong predictor of overall and cardiovascular mortality at 3 years [21]. Secondly, stent protrusion into the aorta could be a serious problem in patients who require surgical intervention in the future. The inability to selectively cannulate coronary vessels prevents antegrade cardioprotection. Stent struts can also make aortic valve replacement surgery extremely difficult. Intraoperative stent trimming poses the risk of deformation of the intracoronary part of the stent [6]. Finally, there is a continuously growing population of patients admitted for transcatheter aortic

valve replacement (TAVR) procedures. In these patients, the protruding stent can be crushed by the delivery balloon or by the valve itself. That risk is best illustrated in Figure 6C, D, where the stent protruding from the LM was crushed by the bulky, calcified valve leaflet during transapical TAVR. The only available arterial access (right radial) was used for pig-tail catheter insertion, preventing LM protection with safety wire and coronary balloon. Despite the patent LIMA-LAD and Ao-Diagonal grafts, the complications turned out to be lethal.

On the other hand, in cases when the operator tries to place the stent precisely, without any protrusion, unintended incomplete coverage of the ostium is common, resulting in a greatly enhanced risk of subsequent restenosis (Fig. 6A, B). In one short series of patients after LM stenting, control MSCT revealed that the stent had been implanted optimally in relation to the ostium only in 3 out of 23 cases [5]. The precise positioning of stents in the coronary ostia is of paramount importance because it can substantially affect long-term clinical success. Unfortunately, angiographic views are plagued with parallax error, and finding a projection orthogonal to the individual aorto-ostial plane is very challenging.

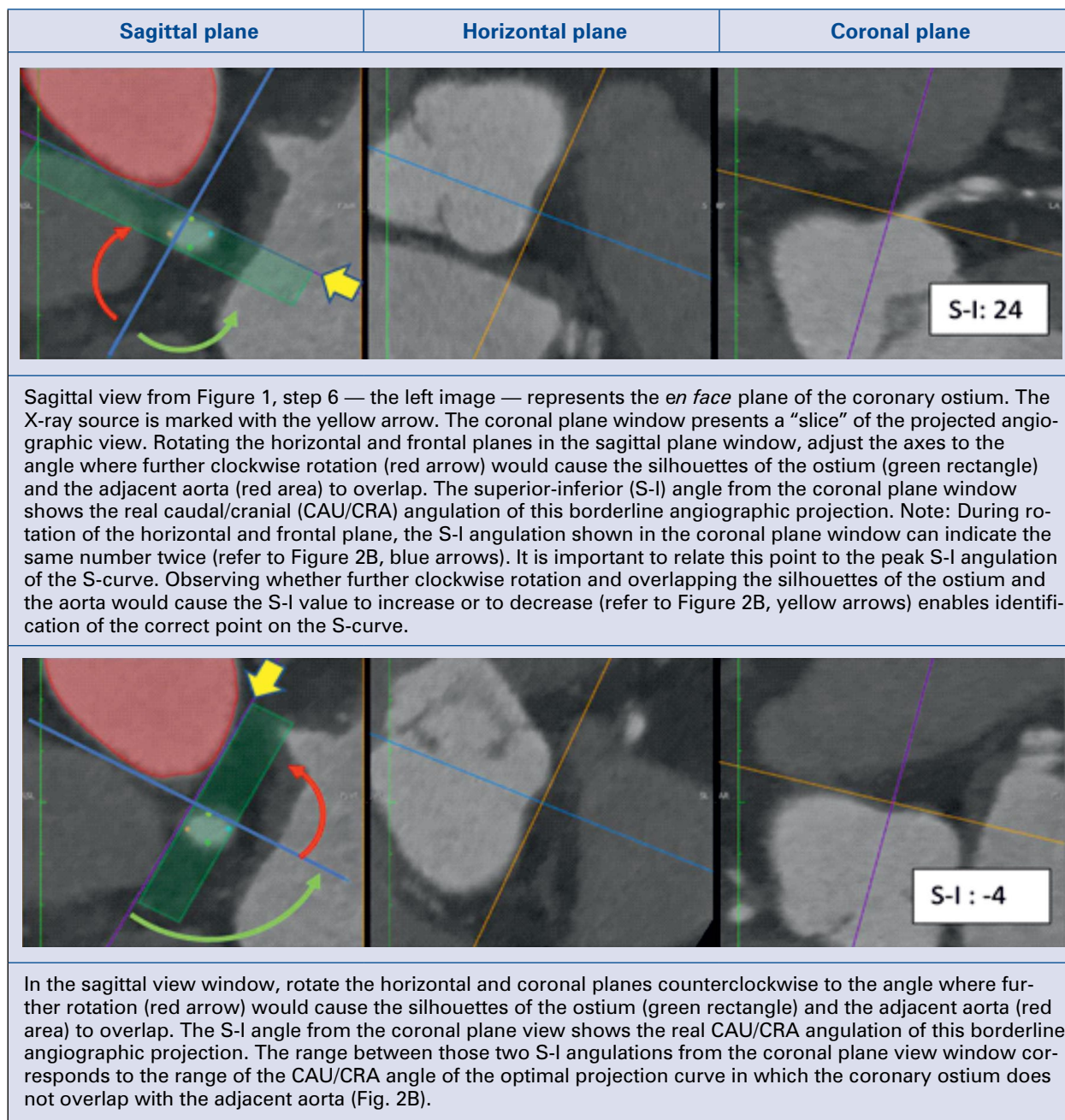


Figure 3. Finding the range of S-curve in which the ostium and the aorta do not overlap with each other.

Table 1. Mean and 95% confidence intervals of *en face* angles of the coronary ostia, and interobserver difference.

| <i>En face</i> view | Overall | Observer 1 | Observer 2 | Difference between observers | Average range of “unobstructed” view |
|---------------------|---|---|---|------------------------------|---|
| LCA ostium | RAO 29; CAU 50 (RAO 24 – RAO 34; CAU 42 – CAU 58) | RAO 28; CAU 49 (RAO 23 – RAO 33; CAU 41 – CAU 57) | RAO 29; CAU 50 (RAO 24 – RAO 34; CAU 42 – CAU 58) | 5 (4–6) | RAO 0 – LAO 68 |
| RCA ostium | RAO 18; CRA 5 (RAO 13 – RAO 23; CAU 2 – CRA 12) | RAO 19; CRA 5 (RAO 14 – RAO 23; CAU 1 – CRA 12) | RAO 18; CRA 5 (RAO 12 – RAO 24; CAU 2 – CRA 12) | 7 (6–8) | RAO 90 – RAO 37 and LAO 48 – LAO 90 |

CAU — caudal angulation; CRA — cranial angulation; LAO — left anterior oblique angulation; RAO — right anterior oblique angulation

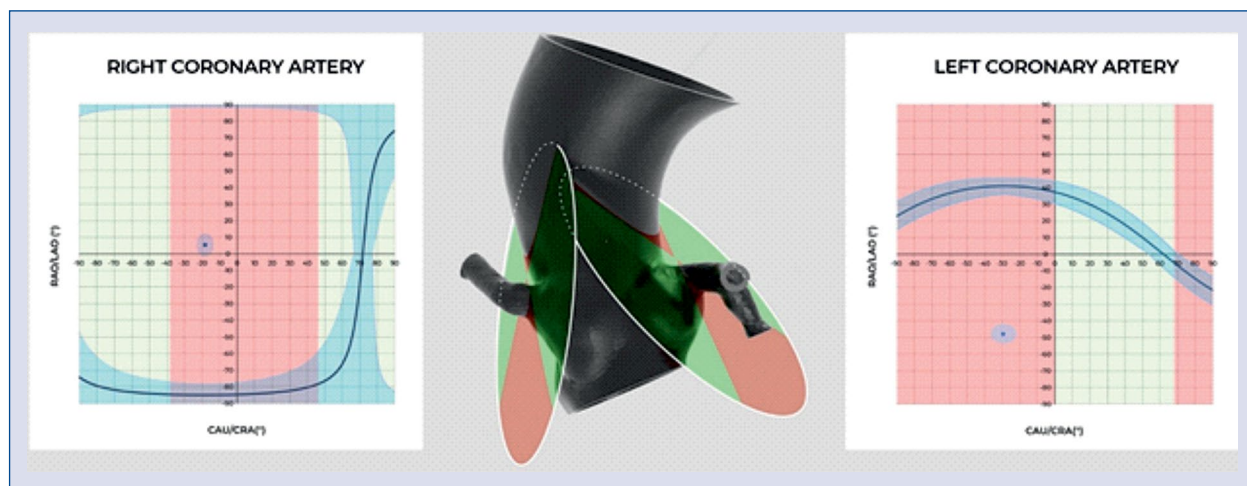


Figure 4. *En face* angles of the right and left coronary ostia and their corresponding optimal projection curves (mean and 95% confidence interval). *En face* angle — blue dot. Optimal projection curve — blue line. The red area indicates the range in which the coronary ostium and the aortic root overlap. Central panel represents schematic illustration of coronary ostia plane in relation to the aortic root.

Accurate image acquisition by using MSCT facilitates PCIs of ostial lesions

Multislice computed tomography provides complete information about the spatial relations between the aortic root, ascending aorta, and coronary vasculature. MSCT data are successfully used for device sizing, procedure planning, and angiographic view optimization during structural cardiac procedures. However, their utilization to facilitate coronary interventions has hitherto been limited, although promising [15, 22]. There are no publications defining an accurate angiographic view for a subsequent coronary procedure based on MSCT image acquisition.

In our study, we propose a simple way of establishing the *en face* angle of the aorto-ostial plane and the corresponding optimal projection curve using a standard DICOM viewer. Results from a group of 30 patients show that the angle of the coronary aorto-ostial plane and its relation to the adjacent aorta are highly variable and patient-specific. In some patients, a large portion of the optimal projection curve of the coronary ostium overlaps with the adjacent aorta, so the range of the “clear” viewing angle is quite limited. In such cases, the ostium is located in the concave part of the aortic root complex (Fig. 7A, C). In other patients in whom the coronary artery has its origin at the convex part of the sinus of Valsalva, it does not overlap with the aorta at any point (Fig. 7B, C). In these scenarios, one should opt for the projection with the smallest CRA/CAU angle.

Taking into account the high variability of coronary ostial planes and aortic configurations, an individual S-curve of the treated ostium should be calculated if an MSCT examination is available. Sometimes in the case of a funnel-shaped ostium, it may be difficult to precisely define anatomical borders. The specific ostium definition can then be fine-tuned according to the planned stenting strategy, i.e. orthogonal to the ostium at the level of the desired stent edge position.

Hitherto, the data regarding the spatial and anatomical location of the coronary ostia in patients admitted for PCI were often not available. However, since MSCT is now a first-line tool for diagnosing CAD in patients with chronic coronary syndromes [23], the availability of these data will be expanding as well. MSCT image interpretation should, therefore, be another skill in the interventional cardiologist’s pocket. Nowadays, PCI operators should not just rely on the radiologist’s report but should also be able to review MSCT exams by themselves, in order to assess anatomical subtleties of every individual patient and optimize the treatment strategy and viewing angles.

However, in most patients admitted for PCI of the LCA or RCA ostium, procedures are performed routinely only based on the clinical experience and judgment of the operator. This also applies to the choice of angiographic projection. The mean *en face* angles and corresponding optimal projection curves from our study roughly reflect current clinical practice. The optimal projection for stenting the

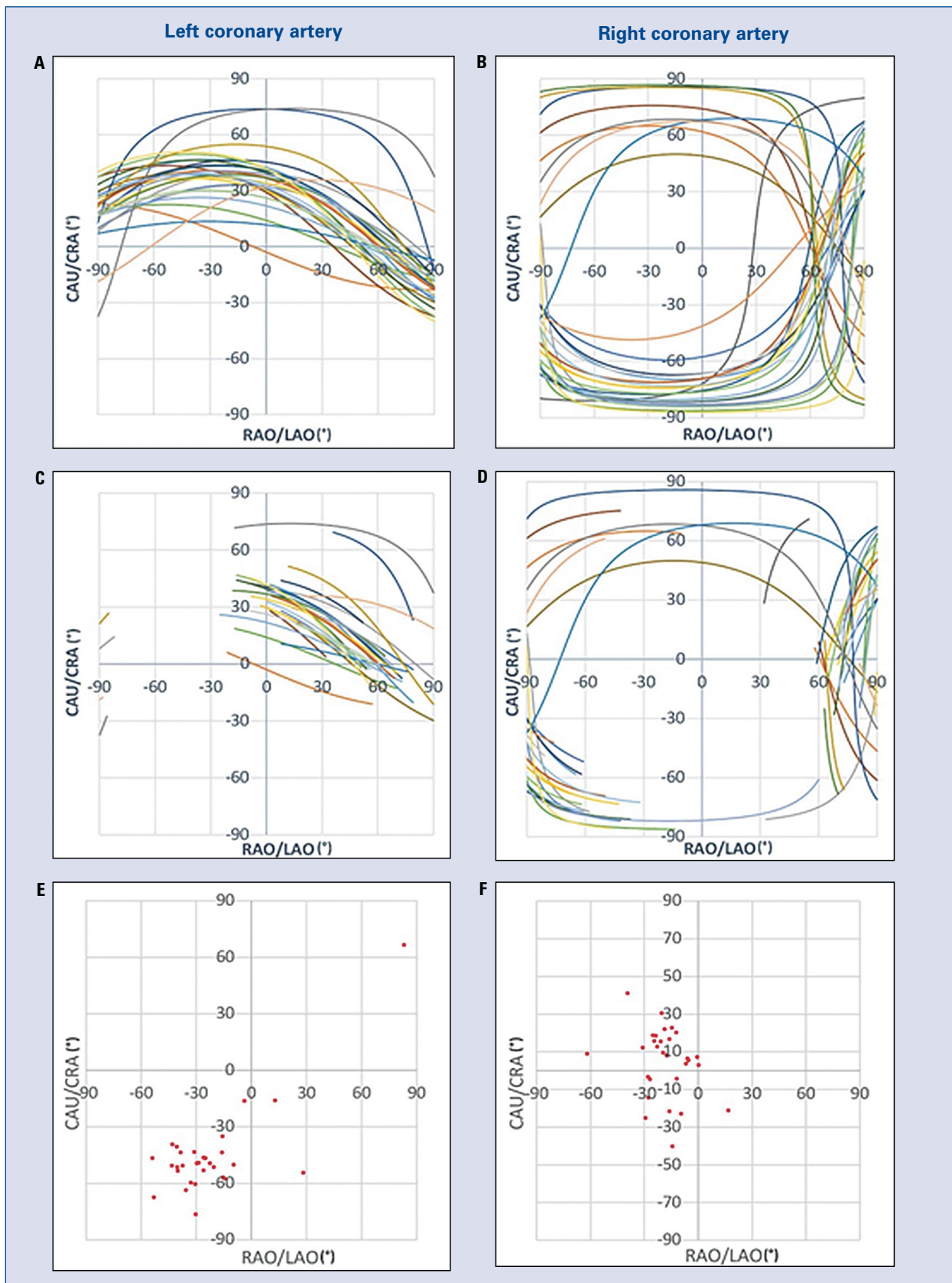


Figure 5. Individual optimal projection curves and *en face* angles in the study cohort. Optimal projection curves for the ostia of the left (A) and right coronary arteries (B). The range of the optimal projection curves in which neither the left (C) nor right coronary ostium (D) overlaps with the adjacent aorta. *En face* angles of left (E) and right coronary ostia (F).

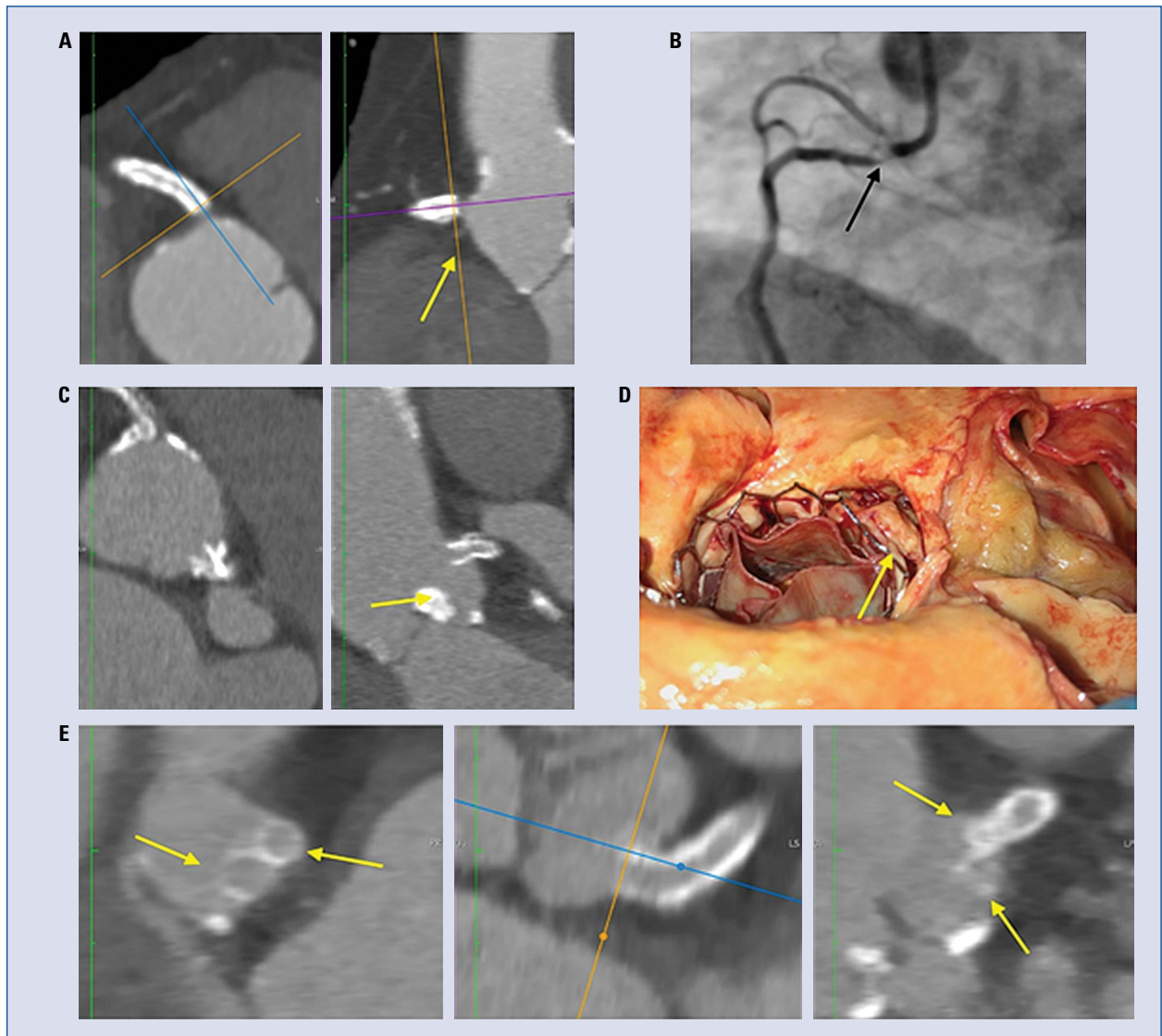


Figure 6. Clinical examples of the suboptimal stent placement in the aorto-coronary ostial lesions. Geographic miss (arrow), stent in the right coronary artery (RCA) implanted too deeply (A); subsequent restenosis in the RCA (arrow) (B); stent protruding from left main into the aorta (arrow) (C); protruding stent crushed (arrow) by the calcified, widened aortic leaflet on postmortem examination (D); two stents protruding from the left coronary artery to the aorta (arrows) accidental finding in the patient admitted for transcatheter aortic valve replacement (E).

LM ostium is usually in the LAO projection with cranial angulation. The best strategy for finding this optimal projection is to start at around LAO 30–40°, CRA 30° and proceed caudally. In the case of the right coronary ostium plane, most optimal projections will be between LAO 60° and 80° with slight cranial angulation. The best strategy seems to be to start in LAO 60°, CRA 10° and then move east toward LAO 90°.

Although two-dimensional (2D) angiographic images are completely spatially unoriented compared to MSCT data, there is a “life hack” solution for finding a projection perpendicular to the

coronary ostium plane. If one aligns the tip of the guiding catheter with the coronary ostium and then finds the projection in which the catheter looks like a straight line with its tip circular, then this corresponds roughly to the ostial plane *en face* angle.

No matter what the CRA/CAU angulation of that ostial plane *en face* angle is, the perpendicular projection will always be located at the position of CRA/CAU 0°, with RAO/LAO angulation equal to the *en face* plane RAO/LAO value plus or minus 90. That may be the starting point for finding the optimal projection and/or calculating the expected/ /approximated S-curve. However, one should keep

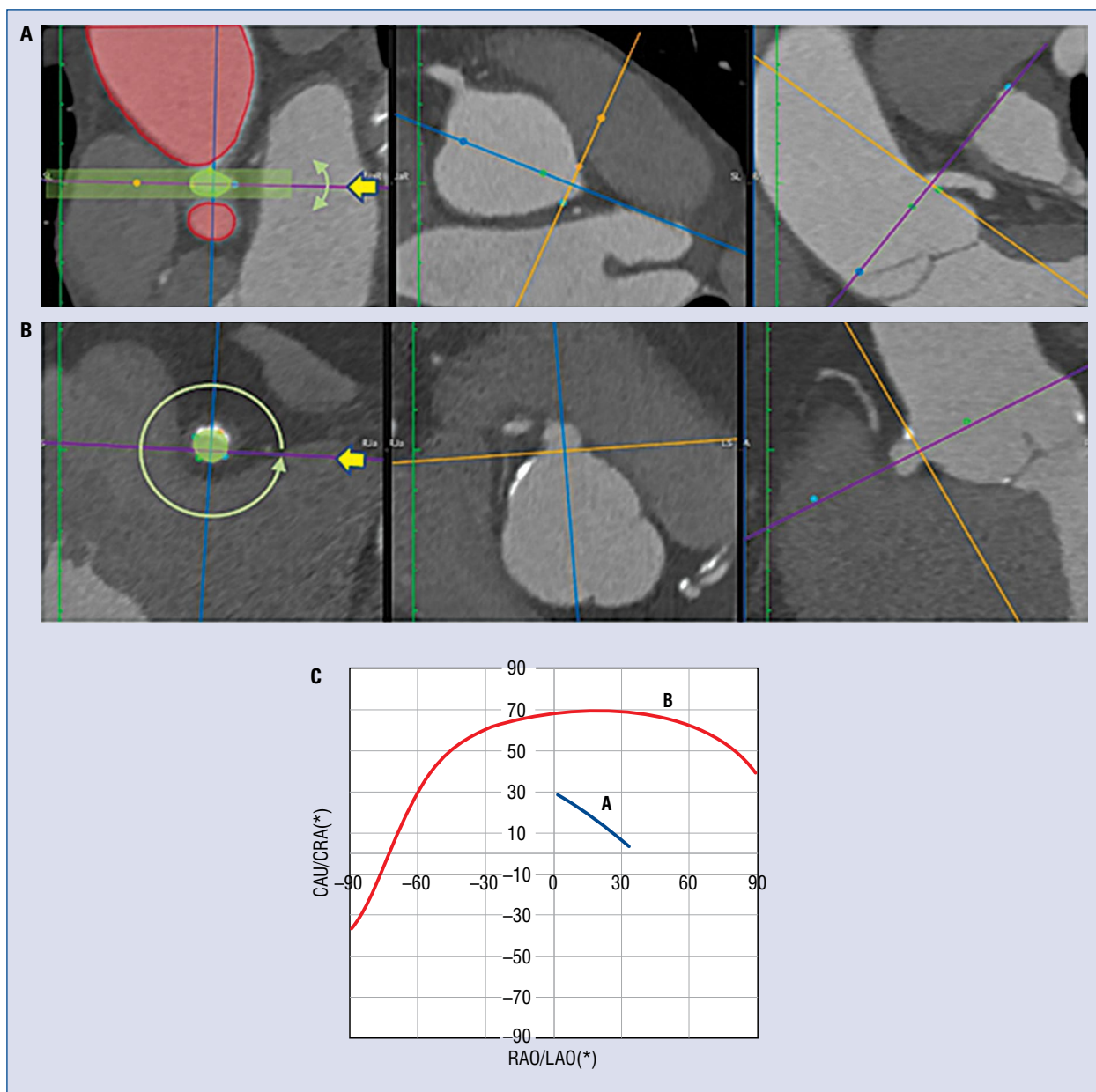


Figure 7. Examples of different aortic root configurations and their impact on the S-curve. Two examples of different aortic root configurations; **A.** A narrow “angiographic window” of the left coronary artery (LCA) ostium (green oval) with a very limited range of possible angulation (green arrow) of the X-ray source (yellow arrow) (adjacent aorta — red area); **B.** A wide “angiographic window” of the right coronary artery (RCA) ostium (green circle), offering a 360-degree view; **C.** The range of the corresponding S-curves in which the coronary ostium does not overlap with the adjacent aorta. In the case of the LCA (blue curve), angiographic viewing angles are limited, but are paradoxically “standard” and easy to achieve, while in the case of the RCA ostium (orange curve), its S-curve is quite atypical and, despite the full range, the degree of cranial angulation in standard left anterior oblique projections makes them unfeasible.

in mind that the tip of the catheter engaged in the coronary ostium is usually oriented upwards. This tendency can be corrected by pushing on the coronary guidewire for better alignment.

Limitations of the study

The main limitation of our study is that the study population consisted of a small group of patients with suspected coronary disease, admitted

for diagnostic CTA, who did not have aorto-ostial lesions, mandating intervention. Thus, the presented data remain experimental. In addition, the data has not been prospectively validated. Third, the method itself is cumbersome. Dedicated software would greatly facilitate the determination of the optimal angle of the coronary ostia. Finally, in the case of structural interventions, a predefined “implantation” projection can easily be corrected during the procedure. This may not be the case with the coronary ostial plane, due to its small size. Altogether, the clinical significance of our method remains to be established.

Conclusions

To overcome the technical challenges of aorto-ostial PCIs, we propose the first systematic step-by-step approach to determine individual fluoroscopic viewing angles for precise stenting by using MSCT image acquisition. The present study shows that, given the substantial variability of the aortic root anatomy, patient-specific implantation angles determined before intervention may essentially facilitate the procedure. The question of whether we should perform MSCT before aorto-ostial PCI for the sake of procedure planning and optimizing its results remains open and needs further prospective investigations.

Conflict of interest: None declared

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